On the hydrodynamic diffusion of rigid particles

O. Gonzalez

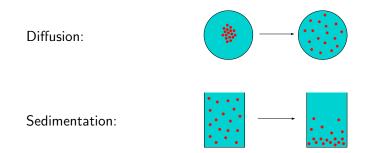
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Application to DNA

Introduction

Basic problem. Characterize how the diffusion and sedimentation properties of particles depend on their shape.



Applications. Molecular separation techniques, structure determination; particle transport, mixing in microfluidic devices.

Spherical bodies

Arbitrary bodies

Asymptotic analysis

Application to DNA



Introduction

Spherical bodies

Arbitrary bodies

Asymptotic analysis

Application to DNA

(Numerical method, if time permits)

Application to DNA

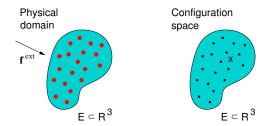
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Spherical bodies

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Classic model for spherical bodies

Setup. Consider a dilute solution of identical spheres in a fluid subject to external loads.



 $\begin{array}{ll} \rho(x,t) & \# \text{ spheres per unit volume of } E. \\ f^{\mathrm{ext}}(x,t) & \text{external body force.} \\ \mu, T & \text{fluid viscosity, temperature.} \end{array}$

Modeling assumptions

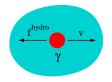
Consider locally time-averaged forces and motion for each particle and assume:

1. Net force balance.



$$f^{\text{ext}} + f^{\text{hydro}} + f^{\text{osmotic}} = 0.$$

2. Hydrodynamic force model.

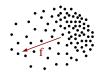


$$f^{\text{hydro}} = -6\pi\gamma\mu\nu$$
, γ radius.

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Modeling assumptions

3. Osmotic force model.



$$f^{\text{osmotic}} = -\nabla \psi, \quad \psi = kT \ln \rho.$$

4. Conservation of mass.



$$\frac{\partial}{\partial t}\int_{B}\rho \, dV + \int_{\partial B}\rho v \cdot n \, dA = 0, \quad \forall B \subset E.$$

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Application to DNA

Resulting model on E

Equations. Combining 1-3 and localizing 4 we get

$$f^{\text{ext}} - 6\pi\gamma\mu\nu - \frac{kT}{\rho}\nabla\rho = 0,$$
 $\qquad \qquad \frac{\partial\rho}{\partial t} + \nabla\cdot[\rho\nu] = 0.$

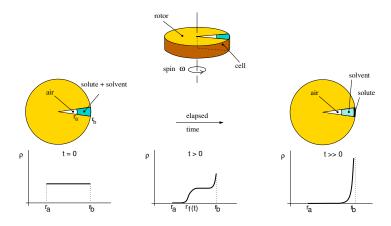
Eliminating v gives

$$\begin{aligned} \frac{\partial \rho}{\partial t} &= \nabla \cdot \left[D \nabla \rho - C \rho f^{\text{ext}} \right] \\ D &= \frac{kT}{6\pi\mu\gamma}, \qquad C = \frac{1}{6\pi\mu\gamma}. \end{aligned}$$

Remark. Various experiments can measure D or C and hence γ .

Application to DNA

Example: centrifuge experiment



D and/or C can be determined from speed of moving front $r_f(t)$.

Arbitrary bodies

Asymptotic analysis

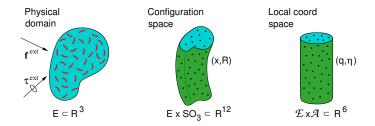
Application to DNA

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Arbitrary bodies

Model for arbitrary bodies

Setup. Consider a dilute solution of identical bodies in a fluid subject to external loads.



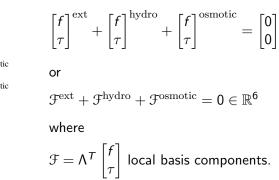
 $\rho(q,\eta,t)$ μ, T

bodies per unit volume of $E \times SO_3$. $(f^{\text{ext}}, au^{\text{ext}})(q, \eta, t),$ external body force, torque. fluid viscosity, temperature.

Modeling assumptions

Consider locally time-averaged loads and motion for each particle and assume:

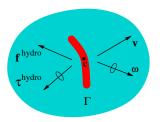
1. Net force and torque balance.



Application to DNA

Modeling assumptions

2. Hydrodynamic force model.



$$\begin{bmatrix} f \\ \tau \end{bmatrix}^{\text{hydro}} = -\begin{bmatrix} L_1 & L_3 \\ L_2 & L_4 \end{bmatrix} \begin{bmatrix} v \\ \omega \end{bmatrix}$$

or
$$\begin{bmatrix} v \\ \omega \end{bmatrix} = -\begin{bmatrix} M_1 & M_3 \\ M_2 & M_4 \end{bmatrix} \begin{bmatrix} f \\ \tau \end{bmatrix}^{\text{hydro}}$$

or
$$\mathcal{V} = -\mathcal{M}\mathcal{F}^{\text{hydro}} \in \mathbb{R}^6$$

where

$$\begin{split} L &= L(\Gamma, c), \quad M = M(\Gamma, c) \in \mathbb{R}^{6 \times 6} \\ \mathcal{M} &= \Lambda^{-1} M \Lambda^{-T}, \quad \mathcal{V} = \Lambda^{-1} \begin{bmatrix} v \\ \omega \end{bmatrix}. \end{split}$$

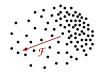
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Application to DNA

Modeling assumptions

3. Osmotic force model.



$$\begin{aligned} \mathcal{F}^{\text{osmotic}} &= -\nabla \psi \\ \psi &= kT \ln \rho, \quad \nabla = (\nabla_q, \nabla_\eta). \end{aligned}$$

4. Conservation of mass.

$$\frac{\partial}{\partial t} \int_{\mathcal{B}} \rho g \, dV + \int_{\partial \mathcal{B}} \rho g \, \mathcal{V} \cdot \mathcal{N} \, dA = 0$$

$$\forall \mathcal{B} \subset \mathcal{E} \times \mathcal{A}.$$

Resulting model on $E \times SO_3$

Equations. Combining 1-3 and localizing 4 we get

$$\mathcal{F}^{\mathrm{ext}} - \mathcal{M}^{-1}\mathcal{V} - \frac{kT}{\rho}\nabla\rho = 0, \qquad \qquad \frac{\partial(\rho g)}{\partial t} + \nabla \cdot [\rho g \mathcal{V}] = 0.$$

Eliminating \mathcal{V} gives

$$\begin{aligned} \frac{\partial \rho}{\partial t} &= g^{-1} \nabla \cdot [g \mathcal{D} \nabla \rho - g \rho \mathcal{C} \mathcal{F}^{\text{ext}}] \\ \mathcal{D} &= k T \mathcal{M}(\Gamma, c), \qquad \mathcal{C} = \mathcal{M}(\Gamma, c). \end{aligned}$$

Remark. Model is fully coupled b/w translations and rotations.

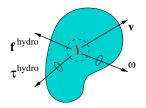
Spherical bodie

Arbitrary bodies

Asymptotic analysis

Application to DNA

Detail on hydrodynamic model

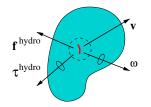


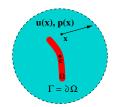
 $\begin{bmatrix} f \\ \tau \end{bmatrix}^{\text{hydro}} = - \begin{bmatrix} L_1 & L_3 \\ L_2 & L_4 \end{bmatrix} \begin{bmatrix} \mathsf{v} \\ \omega \end{bmatrix}$

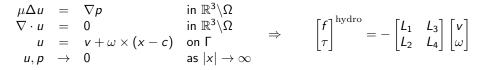
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Application to DNA

Detail on hydrodynamic model







 $M(\Gamma, c) = L(\Gamma, c)^{-1} \in \mathbb{R}^{6 \times 6}$, where $L(\Gamma, c)$ is a Dirichlet-to-Neumann map.

Arbitrary bodies

Asymptotic analysis

Application to DNA

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Asymptotic analysis

Basic question

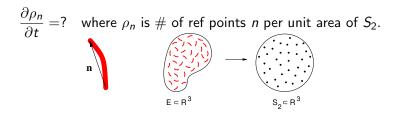
Question. What does the coupled model imply about various observable densities of interest?

 $\frac{\partial \rho_c}{\partial t} = ? \quad \text{where } \rho_c \text{ is } \# \text{ of ref points } c \text{ per unit volume of } E.$

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Basic question

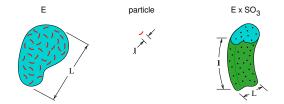
Question. What does the coupled model imply about various observable densities of interest?



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Scale separation

Result. For particles of arbitrary shape, there is a natural scale separation for dynamics on E and SO_3 .



Translations: t_E = time to diffuse across ERotations: t_S = time to diffuse across SO_3

The two-scale structure is ideal setting for asymptotics; the small param is $\varepsilon = \ell/L << 1.$

Limiting model on E

Result. For particles of arbitrary shape Γ and mobility tensor $M(\Gamma, c)$, the leading-order equation on E on the scale t_E is

$$\begin{aligned} \frac{\partial \rho_c}{\partial t} &= \nabla \cdot [D_c \nabla \rho_c - \rho_c h^{\text{ext}}] \\ D_c &= \frac{kT}{3} \operatorname{tr}[M_1(\Gamma, c)], \qquad h^{\text{ext}} = \text{avg ext load} \\ \rho_c &= \# \text{ of ref points } c \text{ per unit volume of } E. \end{aligned}$$



Property of model on E

Result. The diffusivity D_c depends on body shape Γ and ref point c. For each Γ , there is a unique $c_* \in \mathbb{R}^3$ such that

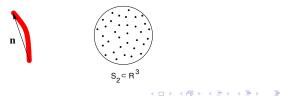
$$D_{c_*} = \min_{c \in \mathbb{R}^3} D_c.$$



Limiting model on S_2

Result. For particles whose shape Γ and mobility tensor $M(\Gamma, c)$ satisfy an elongation condition wrt the body axis n, the leading-order equation on S_2 on the scale t_S is

$$\frac{\partial \rho_n}{\partial t} = D_n \Delta \rho_n$$
$$D_n = \frac{kT}{2} \operatorname{tr}[P_n M_4(\Gamma, c) P_n], \quad P_n = \text{proj orthog to } n$$
$$\rho_n = \# \text{ of ref points } n \text{ per unit area of } S_2.$$



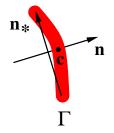
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Property of model on S_2

Result. The diffusivity D_n depends on body shape Γ and ref vector n, but not ref point c. For each Γ , there is at least one $n_* \in S_2$ such that

$$D_{n_*}=\min_{n\in S_2}D_n.$$



Spherical bodies

Arbitrary bodies

Asymptotic analysis

Application to DNA

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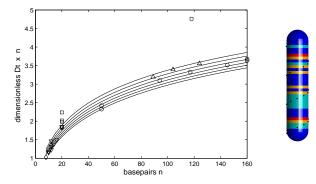
Application

Estimation of hydrated radius

Problem. Given experimental measurements of D_c and D_n for various sequences, we seek to fit the radius parameter r in a geometric model.

 $\Gamma(S, r), S = \text{DNA sequence.}$ r = ? $D_c = \frac{kT}{3} \operatorname{tr}[M_1(\Gamma(S, r), c)], \quad D_n = \frac{kT}{2} \operatorname{tr}[P_n M_4(\Gamma(S, r), c)P_n].$

Results for straight model: D_{c_*} vs sequence length

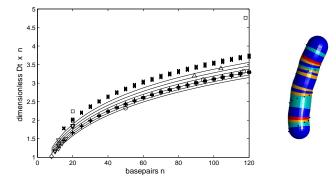


Curves: numerics $w/r = 10, 11, \dots, 15$ Å (top to bottom).

Symbols: experiments (ultracentrifuge, light scattering, electrophoresis). Estimated radius: r = 10 - 15Å.

Application to DNA

Results for curved model: D_{c_*} vs sequence length



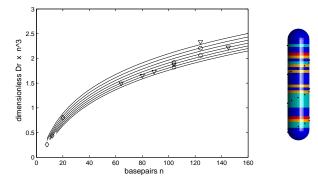
Curves: numerics on straight model (same as before). Open symbols: experimental data (same as before). Crosses, pluses: numerics on curved model w/r = 10, r = 15Å. Estimated radius: r = 12 - 17Å.

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Results for straight model: D_{n_*} vs sequence length



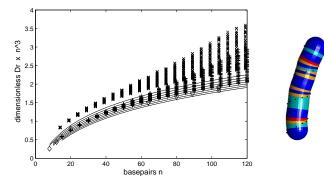
Curves: numerics w/ $r = 12, 11, \ldots, 18$ Å (top to bottom).

Symbols: experiments (birefringence, light scattering).

Estimated radius: r = 13 - 17Å.

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Results for curved model: D_{n_*} vs sequence length



Curves: numerics on straight model (same as before). Open symbols: experimental data (same as before). Crosses, pluses: numerics on curved model w/r = 12, r = 18Å. Estimated radius: r = 10 - 12Å.

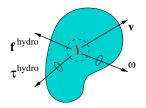
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Numerical method

Application to DNA

Numerical method for $M(\Gamma, c)$

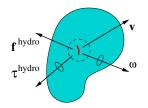


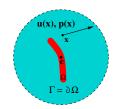
$$\begin{bmatrix} f \\ \tau \end{bmatrix}^{\text{hydro}} = - \begin{bmatrix} L_1 & L_3 \\ L_2 & L_4 \end{bmatrix} \begin{bmatrix} v \\ \omega \end{bmatrix}$$

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Numerical method for $M(\Gamma, c)$





$$\begin{split} & \mu \Delta u &= \nabla p & \text{ in } \mathbb{R}^3 \backslash \Omega \\ & \nabla \cdot u &= 0 & \text{ in } \mathbb{R}^3 \backslash \Omega \\ & u &= U[v, \omega] & \text{ on } \Gamma \\ & u, p &\to 0 & \text{ as } |x| \to \infty \end{split} \Rightarrow \qquad \begin{bmatrix} f \\ \tau \end{bmatrix}^{\text{hydro}} = -\begin{bmatrix} L_1 & L_3 \\ L_2 & L_4 \end{bmatrix} \begin{bmatrix} v \\ \omega \end{bmatrix}$$

The computation of $M(\Gamma, c) = L^{-1}(\Gamma, c) \in \mathbb{R}^{6 \times 6}$ requires six solutions of the exterior Stokes equations with data $U[v, \omega](x) = v + \omega \times (x - c)$.

Application to DNA

Boundary integral formulation

Stokes kernels (singular solns): G(x, y) single-layer, H(x, y) double-layer.

Asymptotic analysis

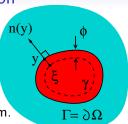
Application to DNA

Boundary integral formulation

Stokes kernels (singular solns): G(x, y) single-layer, H(x, y) double-layer.

Actual, parallel surfaces:

 Γ actual, γ parallel, $0 < \phi < \phi_{\Gamma}$ offset param.



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Asymptotic analysis

Application to DNA

Boundary integral formulation

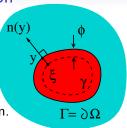
Stokes kernels (singular solns): G(x, y) single-layer, H(x, y) double-layer.

Actual, parallel surfaces:

 Γ actual, γ parallel, $0 < \phi < \phi_{\Gamma}$ offset param.

Mixed representation:

 $\begin{array}{l} u(x) = \lambda \int_{\gamma} G(x,\xi) \psi(y(\xi)) \ da_{\xi} + (1-\lambda) \int_{\Gamma} H(x,y) \psi(y) \ da_{y} \\ 0 < \lambda < 1 \ \text{interpolation param}, \quad \psi \ \text{potential density.} \end{array}$



Asymptotic analysis

Application to DNA

Boundary integral formulation

Stokes kernels (singular solns): G(x, y) single-layer, H(x, y) double-layer.

Actual, parallel surfaces:

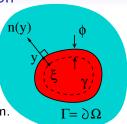
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Integral equation:

Given U find
$$\psi$$
 s.t. $\lim_{\substack{x_o \to x \\ x_o \in \mathbb{R}^3 \setminus \Omega}} u(x_o) = U(x)$ for all $x \in \Gamma$.



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Properties of formulation

$$A^{G}\psi + A^{H}\psi + c\psi = U$$

Integral operators:

$$\begin{aligned} (A^{G}\psi)(x) &= \int_{\Gamma} G^{\lambda,\phi}(x,y)\psi(y) \ da_{y} & \text{regular} \\ (A^{H}\psi)(x) &= \int_{\Gamma} H^{\lambda}(x,y)\psi(y) \ da_{y} & \text{weakly singular.} \end{aligned}$$

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Solvability theorem: Under mild assumptions, there exists a unique $\psi \in C^0$ for any $\Gamma \in C^{1,1}$, $\phi \in (0, \phi_{\Gamma})$, $\lambda \in (0, 1)$ and $U \in C^0$.

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Properties of formulation

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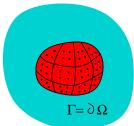
Mobility tensor: Solutions for six independent sets of data are required to determine M.

$$\underbrace{(\mathbf{v},\omega)\longrightarrow U\longrightarrow \psi\longrightarrow (f^{\mathrm{hyd}},\tau^{\mathrm{hyd}})}_{6 \mathrm{ times}}\longrightarrow L\longrightarrow M.$$

Locally-corrected Nystrom discretization

Arbitrary quadrature rule:

 $y_b ext{ nodes}, \quad W_b ext{ weights}, \quad h > 0 ext{ mesh size}, \quad \ell \geq 1 ext{ order}.$



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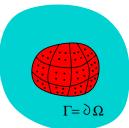
Locally-corrected Nystrom discretization

Arbitrary quadrature rule:

 $y_b ext{ nodes}, \quad W_b ext{ weights}, \quad h > 0 ext{ mesh size}, \quad \ell \geq 1 ext{ order}.$

Partition of unity functions:

$$\zeta_b(x)$$
, $\hat{\zeta}_b(x)$, $\hat{\zeta}_b(x)$, $\zeta_b + \hat{\zeta}_b = 1.$



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Locally-corrected Nystrom discretization

Arbitrary quadrature rule:

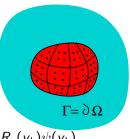
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Partition of unity functions:

$$\zeta_b(x)$$
, $\hat{\zeta}_b(x)$, $\hat{\zeta}_b(x)$, $\zeta_b + \hat{\zeta}_b = 1.$

Discretized operators:

 $\begin{aligned} (A_{h}^{G}\psi)(x) &= \sum_{b} G^{\lambda,\phi}(x,y_{b})\psi(y_{b})W_{b} \\ (A_{h}^{H}\psi)(x) &= \sum_{b} \zeta_{b}(x)H^{\lambda}(x,y_{b})\psi(y_{b})W_{b} + \widehat{\zeta}_{b}(x)R_{x}(y_{b})\psi(y_{b}) \\ R_{x} \text{ local poly correction at } x, \quad p \geq 0 \text{ degree of correction.} \end{aligned}$



 $\Omega G = J$

Locally-corrected Nystrom discretization

Arbitrary quadrature rule:

 $y_b ext{ nodes}, \quad W_b ext{ weights}, \quad h > 0 ext{ mesh size}, \quad \ell \geq 1 ext{ order}.$

Partition of unity functions:

$$\zeta_b(x)$$
, $\hat{\zeta}_b(x)$, $\hat{\zeta}_b(x)$, $\zeta_b + \hat{\zeta}_b = 1.$

Discretized operators: $(A_h^G \psi)(x) = \sum_b G^{\lambda,\phi}(x, y_b)\psi(y_b)W_b$ $(A_h^G \psi)(x) = \sum_b \zeta_b(x)H^{\lambda}(x, y_b)\psi(y_b)W_b + \widehat{\zeta}_b(x)R_x(y_b)\psi(y_b)$ R_x local poly correction at $x, p \ge 0$ degree of correction.

Moment conditions:

 R_x chosen s.t. $A_h^H g = A^H g$ for all local polys g at x up to degree p.

Properties of discretization

$$A^{G}\psi + A^{H}\psi + c\psi = U$$
$$A^{G}_{h}\psi_{h} + A^{H}_{h}\psi_{h} + c\psi_{h} = U$$

Solvability theorem: Under mild assumptions, there exists a unique $\psi_h \in C^0$ for any $\Gamma \in C^{1,1}$, $\phi \in (0, \phi_{\Gamma})$, $\lambda \in (0, 1)$ and $U \in C^0$.



Properties of discretization

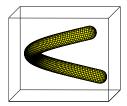
$$A^{G}\psi + A^{H}\psi + c\psi = U$$
$$A^{G}_{h}\psi_{h} + A^{H}_{h}\psi_{h} + c\psi_{h} = U$$

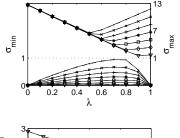
Solvability theorem: Under mild assumptions, there exists a unique $\psi_h \in C^0$ for any $\Gamma \in C^{1,1}$, $\phi \in (0, \phi_{\Gamma})$, $\lambda \in (0, 1)$ and $U \in C^0$.

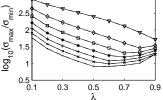
Convergence theorem: Under mild assumptions, if $\Gamma \in C^{m+1,1}$ and $\psi \in C^{m,1}$, then as $h \to 0$

$$\begin{split} ||\psi - \psi_h||_{\infty} &\to 0 & \forall \ell \ge 1, p \ge 0, m \ge 0 \\ ||\psi - \psi_h||_{\infty} &\le Ch & \forall \ell \ge 1, p = 0, m \ge 1 \\ ||\psi - \psi_h||_{\infty} &\le Ch^{\min(\ell, p, m)} & \forall \ell \ge 1, p \ge 1, m \ge 1 \end{split}$$

Conditioning: singular values σ vs parameters λ, ϕ





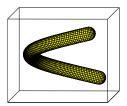


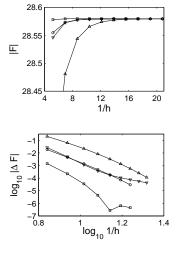
Results for method with p = 0 and $\ell = 1$.

 $\phi/\phi_{\Gamma} = \frac{1}{8}$ (dots), $\frac{2}{8}$ (crosses), $\frac{3}{8}$ (pluses), ..., $\frac{7}{8}$ (triangles). Condition number $\frac{\sigma_{\max}}{\sigma_{\min}} \leq 10^{1.5}$ for $(\lambda, \phi/\phi_{\Gamma})$ near $(\frac{1}{2}, \frac{1}{2})$. ◆□▶ ◆圖▶ ★ 圖▶ ★ 圖▶ / 圖 / のへで

Introduction

Accuracy: computed load f^{hyd} vs mesh size h





Results for method with p = 0 and various ℓ , λ , ϕ .

Convergence is visible; limited by iterative solver.

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